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## 光源面分布对激光针灸经穴组织的漫反射影响

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**摘要:** 为了研究光源面分布对激光针灸经穴组织的漫反射传输影响, 利用激光针灸在穴位组织中虚拟点源的镜像点源分布函数, 并引入格林响应函数, 外推边界条件求解得到点光源的漫射方程解, 由人体穴位4层介质组织的一系列虚拟点源的响应得到不同空间分布光源下人体穴位的激光针灸漫反射模型; 采用蒙特卡罗方法模拟了圆平面、光纤及高斯分布的面光源激光针灸。结果表明, 无光斑时3种光源的径向光能主要集中在近激光针灸点区域, 径向距离大于0.135cm, 3种光源卷积曲线重合, 圆平面和高斯光源的轴向光能呈负指数衰减, 光纤光源呈直线下降; 存在光斑时面光源的漫反射与光斑面积成反比, 等光斑面积下圆屏光斑比圆环光斑的组织漫反射大, 光斑垂直投影处漫反射曲线存在明显畸变, 投影外畸变与距离成反比, 达到0.5个光斑半径距离时畸变基本消除。该结果可为穴位针灸的光源选取与针灸定位提供有益参考。

**关键词:** 医用光学与生物技术; 面光源针灸; 蒙特卡罗; 漫反射

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### Diffuse reflection on the acupuncture point under laser acupuncture with different spatial distribution

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**Abstract:** In order to study the diffuse transmission influence of laser acupuncture with different surface distribution light sources, the image-point-source distribution on meridian tissue is analyzed and diffusion equation of the image-point-source is solved through the use of extrapolation boundary conditions and Green response. Diffuse output models in acupuncture region for different distribution surface light source are obtained by a series responses of virtual points source. Flat, fiber and gauss acupuncture laser are simulated by Monte-Carlo method. The results indicated that: (1) the radial light energy in three acupuncture without spot mainly was concentrated in the near light source region and coincided when the radial distance to more than 0.135cm, and axial light energy showed a negative exponential decay in flat and gauss acupuncture and linear decline in fiber source; (2) when surface light source existed circular or ring spot, the diffuse was inversely proportional to the spot area, especially the diffuse of circular spot being larger than the ring spot under the same spot area, and diffuse reflectance curve had a significant distortion at the vertical projection and was inversely proportional to the distance outside the projection, especially when the distance to 0.5 times of the spot radius the curve distortion being basically eliminated. The results may provide a useful reference for light source selection and acupuncture location of acupuncture points.

**Key words:** medical optics and biotechnology; surface laser acupuncture; Monte-Carlo; diffuse reflection

## 引言

近年来,应用激光针灸照射穴位代替传统针灸以达到镇痛和治疗的研究已得到生物学界的广泛重视<sup>[1-4]</sup>。激光针灸照射到穴位时,通过正常的反射、折

射、吸收及散射等过程达到一定深度的相应治疗点,在激光电磁场的作用下使细胞电兴奋产生一动作电位,起到最佳的生物效应和针灸刺激作用。激光电场不仅仅取决于生物组织的光学特性、作用时间和方向的影响,还受激光光源的能量密度大小、光源空间分布和光斑面积及形状的影响。目前的激光针灸研究主要以低强度无限细笔型光束单点入射或聚焦面光源照射穴位治疗区域,而针对不同空间面分布的激光光源研究较少。鉴于此,作者首先给出了激光针灸在穴位组织中虚拟点源的镜像点光源分布函数;然后引入格林响

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应函数,利用外推边界条件求解得到点光源的漫射方程解,由人体穴位4层介质组织的一系列虚拟点源的响应得到不同空间分布面光源下人体穴位的激光针灸漫反射模型;最后利用蒙特卡罗法给出了不同空间分布面光源激光针灸下穴位治疗区域组织的漫反射仿真结果。

## 1 穴位4层介质的激光针灸漫反射响应模型

人体穴位组织是具有分层特性的生物组织。一些腧穴组织学研究观察的资料表明,穴位组织介质可分为表皮、真皮、皮下组织(主要成分为脂肪)和肱桡肌4个同心层,每一层具有相同的光学特性和热效应。中医针灸治疗区域主要在肱桡肌层,激光针灸照射到穴位时,需通过前3层介质的反射、折射、吸收及散射等过程后达到治疗区域层<sup>[5]</sup>。

假定单色连续入射光束半径范围内的光强是恒定的,光束范围外的光强为0,激光针灸入射的每条光线对应的虚拟点源分布函数 $\varepsilon(\mathbf{r},s,t)$ 与入射的面光源有关,虚拟点源位置 $\mathbf{r}$ 为:

$$\mathbf{r} = \mathbf{r}_{z=z_i'} + s \times 3D_i \quad (1)$$

式中, $D_i = \{3[\mu_{a,i}(1-g_i) + \mu_{s,i}]\}^{-1}$ , $D_i$ 为第*i*层等效各向同性散射系数, $\mu_{a,i}$ 、 $\mu_{s,i}$ 和 $g_i$ 依次为第*i*层的吸收系数、散射系数和各向异性因子, $i=1,2,3,4$ , $\mathbf{r}_{z=z_i'}$ 为光线在入射面上的位置, $s$ 为光线的传播方向。

虚拟点源的能量分布处于与时间无关的稳定状态,满足漫射方程:

$$D_i \Delta \Phi_i(\mathbf{r}) - \mu_{a,i} \Phi_i(\mathbf{r}) + Q_i(\mathbf{r}) = 0 \quad (2)$$

式中, $\Phi_i(\mathbf{r}) = \int_{4\pi} S_i(\mathbf{r},s) d\Omega$ 。 $\Phi_i(\mathbf{r})$ 为第*i*层的能流率, $S_i(\mathbf{r},s)$ 为第*i*层的约化入射强度与介质外进入的漫射光强之和。考虑到介质层折射率不匹配,根据外推边界条件<sup>[6]</sup>,在穴位组织介质外引入镜像光源 $S_i'(\mathbf{r},z)$ ,与虚拟点光源方向相反,光源的大小表示为:

$$S_i'(\mathbf{r},z) = S_i(0,z_i) - S_i[0, -(2z_b + z_i)] \quad (3)$$

式中, $z_b = \frac{1+R_{\text{eff}}}{1-R_{\text{eff}}} 2D_i$ , $R_{\text{eff}}$ 为光在边界处的内部反射率。

将镜像点光源函数与自由边界条件下漫射方程的格林函数解进行卷积,得到穴位第*i*层介质的点光源的漫射方程解为:

$$\Phi_i(\mathbf{r},z) = \frac{1}{4\pi D_i} \times \left[ \frac{1}{r_1} \exp\left(-\sqrt{\frac{\mu_{a,i} r_{1,i}^2}{D_i}}\right) - \frac{1}{r_2} \exp\left(-\sqrt{\frac{\mu_{a,i} r_{2,i}^2}{D_i}}\right) \right] \quad (4)$$

式中, $r_{1,i} = \sqrt{r^2 + (z-z_i)^2}$ , $r_{2,i} = \sqrt{r^2 + (z+z_i+2z_b)^2}$ 。在通常的激光针灸应用中,生物组织的横向尺寸一

般远大于入射光束直径,人体组织可看成是一个线性的平移不变系统,因此,外部激光光源照射条件可以等价于层状生物组织内部一系列虚拟点源的响应<sup>[7]</sup>,即可得到激光面光源在穴位各层组织的漫反射响应为:

$$\Phi_i(\mathbf{r},s,t) = \iiint_V \varepsilon(\mathbf{r}',s,t) \Phi_i(\mathbf{r},\mathbf{r}',s,t) d\Omega \quad (5)$$

## 2 仿真实验及结果讨论

蒙特卡罗模型通过相应的概率模型和随机数发生器产生的随机数来模拟单个光子在介质中的行走过程,是一个广泛应用且较为理想的方法<sup>[8-10]</sup>。作者用蒙特卡罗法分别模拟了在均匀分布的圆平面光束、光纤传导以及高斯光束等激光针灸照射下,人体手阳明大肠经曲池穴的治疗区域的漫反射强度分布。

对于不同特性的光束,蒙特卡罗法模拟时的初始条件不同。对于均匀分布的圆平面光束垂直入射组织表面的某一范围,可认为此范围细分的每个网格里存在同样初始条件的蒙特卡罗模拟;垂直入射表面的高斯光束的入射范围内所有网格的光子权重分布则满足高斯分布;而对于光纤光束来说,由于有一定的数值孔径,光子的初始方向不同,其光子权重随初始方向的不同有一个角分布。光源光斑用在2维网格上挡去不同的部分的方法获得。

人体曲池穴的组织介质为半无限介质,中医针灸治疗区域主要在肱桡肌层,中心针灸点深度为 $(4.4 \pm 0.3)$ cm。穴位组织各层的光学参量<sup>[11]</sup>见表1。

Table 1 Optical parameters of each story in the Quchi tissue

tissue layer	$\mu_a/\text{cm}^{-1}$	$\mu_s/\text{cm}^{-1}$	$n$	$g$	$L/\text{cm}^{-1}$
epidermis	4.3	107	1.43	0.78	0.07
dermis	2.8	196	1.41	0.82	0.73
subcutaneous	3.6	213	1.46	0.83	3.20
brachioradialis	5.4	315	1.39	0.82	—

假定光源入射波长为632nm,光束半径为0.1cm,入射光在肱桡肌层治疗区域的表面中心作为坐标原点,厚度方向为 $z$ 坐标,平行于层面方向为 $r$ 坐标,与 $z$ 轴的夹角为 $\theta$ 。为获得足够的精度,跟踪的光子数取100万个,单位网格 $\Delta r$ 和 $\Delta z$ 均为0.01cm。

### 2.1 无光斑时、不同面光源的激光针灸情况下

图1为无光斑时、3种激光束针灸情况下,曲池穴肱桡肌层中治疗中心点所在横截面的漫反射随径向距离 $r$ 以及中心线上轴向漫射分布的模拟结果。

由图1a可见,3种光源的光能流率和漫反射强度的径向分布主要都集中在近激光针灸点区域,与光源半径有关。均匀分布光源在近激光针灸点区域的径向漫反射强度比较均衡,曲线平稳。高斯面光源变化曲

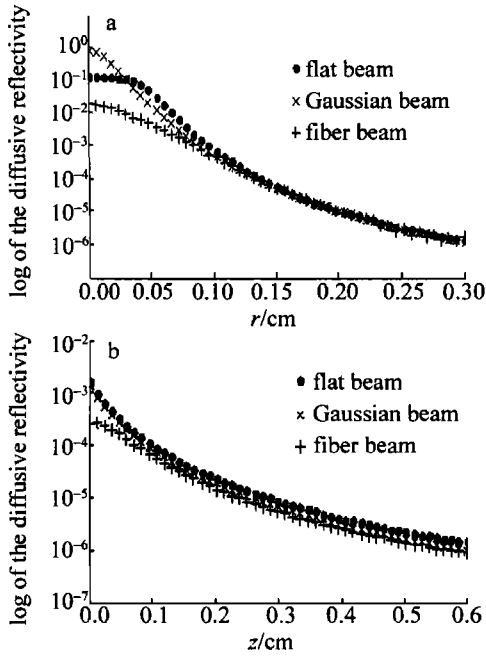


Fig. 1 The diffusive reflectivity distribution of Quchi acupoint therapy area with different surface light source  
a—radial distribution b—axial distribution

线比较陡峭,漫反射曲线变化大。光纤光源的曲线变化平缓,在整个治疗区域的漫反射受径向距离影响小。当径向距离达到 0.135cm 时,3 种光源产生的卷积曲线几乎重合,光能流率和漫反射强度对面光源特性的依赖性小。当径向距离大于 0.236cm 时,光纤传导的光源漫反射信号出现波动,易受随机光子吸收数和组织吸收系数的影响,可通过增加跟踪的光子数和增加光源半径来提高。由图 1b 可见,3 种光源漫反射强度越远离肱桡肌层介质表面漫反射越小,高斯光束和圆平光束的光能流率随  $z$  的变化基本是按负指数衰减,光纤光源呈直线下降,但高斯光束的光能流率随  $z$  的变化比圆平面光束和光纤光源陡。以上结论与入射波长为 904nm 的模拟结论基本相符。结果表明,高斯分布面光源照射下,光源的形状对于漫反射率的影响主要在于距离光源较近的区域,在远离光源的区域受光源的形状变化以及探测器的性能影响较小。

2.2 在不同光斑大小、不同面光源情况下

图 2 为存在圆环光斑或圆屏光斑时,3 种激光束针灸在曲池穴肱桡肌层的治疗区域中径向漫反射光能分布的模拟结果。图 2 中  $R_{r,s}$ ,  $R_{c,s}$  分别表示圆环光斑的内径和圆屏光斑的半径,当  $R_{r,s} = R_{c,s}$  时,两种光斑面积相等。

由图 2 可见,圆屏光斑和圆环光斑下,空间分辨漫反射随光斑面积的增大而变小,相同光斑面积下圆屏光斑比圆环光斑的组织漫反射大。光斑垂直投影治疗区域内的组织漫反射曲线存在明显畸变,区域外越远离光斑时穴位组织漫反射所受的影响越小,当距离大

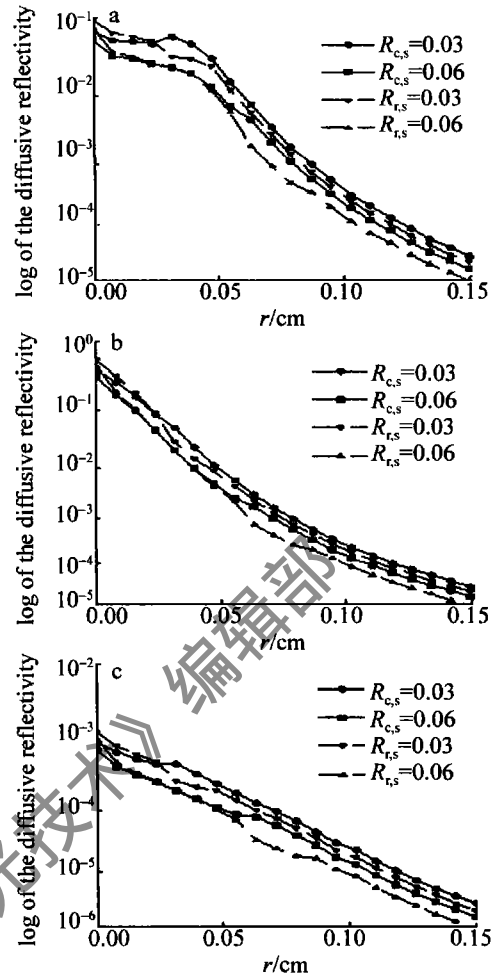


Fig. 2 Variation of diffusive reflection with radial distance  
a—flat beam b—fiber beam c—Gaussian beam

于 0.5 个光斑半径时,光斑的影响基本消除。从图中还看出,光斑对均分分布面光源激光针灸的漫反射影响最大,光纤光源次之,高斯光源最弱,这表明在中医激光针灸应用中,可通过改变光斑大小及形状来对针灸位置进行定位。

3 结论

作者从穴位分层介质的漫射方法出发,利用卷积给出了不同空间分布面光源下激光针灸穴位的漫反射方程解。利用蒙特卡罗法模拟了不同空间分布和不同光斑分布的面光源激光针灸。结果表明,光源形状及大小对激光针灸的影响主要集中在近光源区域,远离光源区域外,漫反射光能和光能流率都变得较弱,并且随着径向和轴向尺寸的增大而迅速衰减;光斑对激光针灸的影响主要集中在光斑垂直投影治疗区域内,光斑对均分分布面光源激光针灸的漫反射影响最大,光纤光源次之,高斯光源最弱。因此,实际应用中可根据穴位区域大小、位置来选择合适光源和光斑,通过调整光源的空间分布,改变光斑大小及位置来研究激光针

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灸穴位区域组织的漫射率等组织特性及对针灸位置进行定位,对现在的经络研究有特别意义,可为深入研究人体经络特性提供基础。

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